Development of Sustained Release Eudragit Based Matrix Tablet of Fluvastatin Sodium Microspheres

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The purpose of this research is to investigate the suitability of acquiring improved dissolution profile and sustained release of Fluvastatin sodium to reduce dosage frequency via a novel combination of freeze dried microspheres and Eudragit polymers-based matrix tablet technologies. Fluvastatin sodium microspheres were prepared using polyvinyl pyrollidone K-30 and Poloxamer 407 through solvent evaporation via freeze drying. We adopted a central composite design to examine the influence of independent variables viz. drug:polymer (X1) and surfactant (X2) on the t50% (Y1), Q90 (Y2) and percentage drug content (Y3) along with determination of an optimized composition for production of an optimal Fluvastatin sodium microspheres. Design expert software illustrated that an optimized Fluvastatin sodium microspherescould be achieved using 1:3.496 drug:polymer and 3.102 % poloxamer 407 which would illustrates t50% (36.33 min), Q90 (79.99 %) and percentage drug content (81.589 %). The mean diameter and polydispersity index of Fluvastatin sodium microspheres using dynamic light scattering was found 0.78 µm and 0.287, respectively. Sustained release tablet of optimized Fluvastatin sodium microspheres (Fluvastatin sodium microspheres-sustained release tablet) was manufactured using Eudragit RS 100 and Eudragit RL 100 based granules by wet granulation technique. In vitro drug release kinetics studies were executed to assess the drug release mechanism from optimized Fluvastatin sodium microspheres and Fluvastatin sodium microspheres-sustained release tablet. The dissolution level of Fluvastatin sodium was 3.58-fold improved within 2 h through the freeze dried microspheres. Fluvastatin sodium microspheres-sustained release tablet showed sustained drug release over 24 h and was matched properly to Korsmeyer-Peppas model with release exponent of 0.5318, which indicated drug release through diffusion and erosion mechanism. Conclusively, it has been demonstrated that novel combination of freeze dried microspheres and their Eudragit polymers-based matrix tablet techniques could find great potential for improving drug dissolution and sustained release of water insoluble drugs along with reduced dosage frequency.

Key words: Microspheres, matrix tablet, central composite design, polyvinyl pyrollidone K-30, Poloxamer 407, Eudragit RS 100, Eudragit RL 100, Korsmeyer-Peppas

Oral route is generally viewed as the most comfortable and convenient route for medication. Absorption of oral dosage in the aqueous gastrointestinal fluid varies depending on their requisite solubility. It has been reported that approximately 40 % of existing and newly manufactured drug molecule undergo low solubility and dissolution characteristics. Due to their slow and constrained release into gastrointestinal fluid causing low oral bioavailability; poor water solubility of drugs has become one of the biggest concerns in pharmaceutical formulations[1,2]. Numerous approaches such as nano-suspensions[3], nano-structured lipid carriers[4] and solid dispersion[5] have been utilized for improving dissolution of Fluvastatin Sodium (FLS). However, no attempt has been made for developing FLS microspheres; however microspheres have tremendous potential to augment the dissolution of class II drugs[6,7]. Since, FLS is Biopharmaceutical Classification System (BCS) class II drug having poor aqueous solubility and therefore reduced drug dissolution and low (24 %) oral bioavailability. Therefore, there is requisite

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of improving dissolution of FLS. Therefore, in present investigation, solvent-evaporation technique followed by freeze-drying has been utilized for production of Fluvastatin Sodium Microspheres (FLS-MS). It is an advanced solvent removal technology with tremendous prospective in the pharmaceutics for conversion of active pharmaceutical ingredient from the crystalline to amorphous form, production of microspheres with prompt hydration potential. In this process, moisture is removed from the product via sublimation as well as desorption phase\textsuperscript{[8]}. The hydrophilic excipients i.e. Polyvinyl Pyrollidone K-30 (PVP K-30) and Poloxamer 407 has been used in microsphere production which plays an imperative function in enhancing drug’s wettability, dispersibility and dissolution\textsuperscript{[7]}. PVP K-30 is a biocompatible hydrophilic amorphous polymer having low toxicity, high aqueous solubility, economic cost and physiological tolerance which has been recognized as safe by the Food and Drug Administration\textsuperscript{[9-11]}. Poloxamer 407 is poloxystyrene-polypropylene block copolymer nonionic surfactant that has good solubilizing capacity, low toxicity, good drug-release characteristics and can achieve the highest degree of dissolution enhancement\textsuperscript{[12]}. Central Composite Design (CCD) was explored to execute the experimentation for microsphere production and for selection of an optimal composition of optimized FLS-MS for achieving the maximum percentage drug dissolution along with the least number of experiments\textsuperscript{[13]}. Another shortcoming of FLS is short half-life (1-3 h) and oral dosage regimen of 40 mg capsule twice daily. Therefore, once-daily sustained-release tablet of FLS is desirable which could provide a more constant plasma concentration with improved patient compliance. In sustained-release technology, hydrophilic matrix materials i.e. Eudragit RS 100 (low permeability) and Eudragit RL 100 (high permeability) exhibiting pH independent swelling has been utilized for manufacturing of Sustained Release Tablet (SRT) of optimized FLS-MS (having improved dissolution) (FLS-MS-SRT)\textsuperscript{[14-17]}. The aim of the present study was to explore novel combinations of freeze dried microspheres and their Eudragit polymers-based matrix tablet techniques in an attempt to improve drug dissolution and develop once-daily sustained-release matrix tablet of optimized FLS-MS, respectively.

MATERIALS AND METHODS

Materials:

Fluvastatin sodium (CAS-No: 93957-55-2) was provided by All Well Pharmaceuticals Company, Chandigarh, India. Polyvinyl pyrollidone K-30 was purchased from Loba Chemicals (Mumbai, India). Poloxamer 407 was obtained from Oniosome Healthcare Private Limited, Mohali, India. Evonik Industries AG-Mumbai (India) supplied Eudragit RL 100 and RS 100. All other chemicals were of analytical grade.

Central composite design layout for production of FLS-MS:

The 13 batches of FLS-MS were manufactured according to CCD layout given by Stat-Ease Inc Design Expert\textsuperscript{®} Software (Version 11.0.4.0) for assessing the influence of two important factors-drug:polymer (X1) and surfactant (X2) on the t\textsubscript{50} (min) (Y1), Q\textsubscript{90} (percent) (Y2) and drug content (percent) (Y3) along with determination of an optimized composition for production of an optimal FLS-MS (Table 1).

Preparation of FLS-loaded solvent-evaporated microspheres:

FLS-MS were fabricated by solvent evaporation technique followed by freeze drying. Briefly, accurately weighed quantity of FLS was dissolved in acetone (10 ml) while PVP K-30 and Poloxamer 407 were dissolved in distilled water (20 ml). The organic phase was transferred slowly into aqueous phase while continuous magnetic stirring at 1500 rpm for 45 min.

<table>
<thead>
<tr>
<th>Run number</th>
<th>Drug: polymer (w/w) (X1)</th>
<th>Surfactant (percent w/v) (X2)</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>-1 (1:2)</td>
<td>-1 (1)</td>
</tr>
<tr>
<td>2</td>
<td>1 (1:4)</td>
<td>-1 (1)</td>
</tr>
<tr>
<td>3</td>
<td>-1 (1:2)</td>
<td>1 (3)</td>
</tr>
<tr>
<td>4</td>
<td>1 (1:4)</td>
<td>1 (3)</td>
</tr>
<tr>
<td>5</td>
<td>-1.41 (1:1.59)</td>
<td>0 (2)</td>
</tr>
<tr>
<td>6</td>
<td>1.41 (1:4.41)</td>
<td>0 (2)</td>
</tr>
<tr>
<td>7</td>
<td>0 (1:3)</td>
<td>-1.41 (0.59)</td>
</tr>
<tr>
<td>8</td>
<td>0 (1:3)</td>
<td>1.41 (3.41)</td>
</tr>
<tr>
<td>9</td>
<td>0 (1:3)</td>
<td>0 (2)</td>
</tr>
<tr>
<td>10</td>
<td>0 (1:3)</td>
<td>0 (2)</td>
</tr>
<tr>
<td>11</td>
<td>0 (1:3)</td>
<td>0 (2)</td>
</tr>
<tr>
<td>12</td>
<td>0 (1:3)</td>
<td>0 (2)</td>
</tr>
<tr>
<td>13</td>
<td>0 (1:3)</td>
<td>0 (2)</td>
</tr>
</tbody>
</table>
to remove organic solvent. Subsequently, samples were lyophilized in freeze dryer (Allied Frost, New Delhi) at 
-70° and 0.05 kPa vacuum for 24 h to acquire fine FLS-
MS powder. Subsequently, microspheres desiccated for 
48 h to eliminate the remaining moisture[8,18-20].

Evaluation of response parameters for Fluvastatin 
sodium microspheres:

Determination of t _50 % (Y1) and Q90 (Y2): In vitro 
FLS release from FLS-MSs was examined using United 
States Pharmacopeia (USP) dissolution apparatus (type 
II) (Lab India, Mumbai) (900 ml phosphate buffer pH 
6.8, 100 rpm at 37°, n=3). Samples were collected at 
specified intervals and quantities of the drugs were 
analyzed using Systronics ultraviolet spectrophotometer 
(Model: AU-2701) (Fluvastatin sodium λ=300 nm). 
From in vitro drug release graph plotted between 
Percentage Cumulative Drug Release (% CDR) and 
time (min), t _50 % which corresponds to the time taken 
for fifty percent CDR and Q90 which correspond to the 
percentage CDR within 90 min were determined[21].

Determination of percentage drug content (Y3):

Accurate quantity of FLS-MS (10 mg FLS) was 
dissolved in 10 ml phosphate buffer (pH 6.8), analyzed 
through spectrophotometer and percentage drug content 
determined using following equation[22]:

\[
\text{Percentage drug content} = \frac{\text{Actual amount of Fluvastatin sodium}}{\text{Theoretical amount of Fluvastatin sodium}} \times 100
\]

Graphical optimization and validation of optimized 
FLS-MS:

An overlay plot was developed using graphical 
optimization tool in Design-Expert software to 
acquire graphical view displaying optimum values 
of independent factors (coded values of X1 and X2) 
and predicted response variable (Y1, Y2 and Y3). 
To validate the graphical optimization, an additional 
experimental batch of FLS-MS was manufactuated 
using optimal variables values and in vitro dissolution 
was performed for estimating t _50 % (Y1) and Q90 (Y2) 
and percentage drug content (Y3). For fulfilling the 
validation strategy, the experimental values of response 
variables should be in close agreement with software 
predicted values[13].

Characterization of optimized FLS-MS:

Fourier-transform infrared spectroscopy (FTIR):

FTIR spectra of FLS, PVP K-30, Poloxamer 407, drug- 
polymers Physical Mixture (PM) and FLS-MS were 
obtained using FTIR spectrometer (Bruker, Model: 
Alpha-T, software: OPUS) to confirm drug-polymer 
compatibility and entrapment of FLS in microspheres. 
The sample prepared using potassium bromide by 
hydraulic press method was analyzed from 4000 to 
400 cm⁻¹.

Powder X-Ray Diffraction (PXRD) analysis:
The PXRD patterns of FLS, PVP K-30, Poloxamer 407, PM 
and optimized FLS-MS were obtained using XPERT-
PRO x-ray diffractometer. The samples were scanned 
at 2θ angle over 5-50° at 40 mA and 45 kV using 
Copper K-Alpha (CuK-α) (1.54 Å) and CuK-bBeta (β) 
(1.39 Å) radiations.

Dynamic light scattering:

Mean diameter and 
Polydispersity Index (PDI) for particle size distributions 
of optimized FLS-MS were estimated by dynamic light 
scattering technique using Beckman Coulter, Version 
3.73/2.30 (USA). In brief, 20 mg of FLS-MS was 
dispersed in 2 ml of distilled water in quartz cuvette 
and measurements were carried out at 25°.

Scanning Electron Microscopy (SEM):
The morphological properties and shape of freeze dried 
optimized FLS-MS was recorded using Jeol JSM6100 
(Japan). Sample was located on aluminium stub 
utilizing double-sided adhesive tape and examined at 
1.4 kV subsequent to 20 nm gold films coating through 
sputtering.
Preparation of FLS-MS-SRT:

Eudragit based granules were prepared using mixture of lactose, Eudragit RS 100, Eudragit RL 100 and magnesium stearate. The powder blend was granulated using polyvinyl alcohol binder solution in ethanol:water (20:80) to produce wet mass which was screened through #44 sieves and dried to obtain uniform size granules. Finally, Eudragit based granules, FLS-MS and talc were blended and compressed into tablets (600±10 mg) using single punch tablet press (AK industries, Nakodar)[16,26-28].

In vitro drug release profile and release kinetics (FLS-MS vs. FLS-MS-SRT):

The in vitro drug release from FLS, PM, FLS-MS and matrix tablets (FLS-MS-SRT) was investigated using USP paddle dissolution equipment as described previously. To explore the drug release process, data were incorporated into zero order, first order, Higuchi model as well as Korsmeyer-Peppas model. The release constant (K) and regression coefficient values (r²) were calculated for all the models. Drug release mechanism from FLS-MS and FLS-MS-SRT was explored using release exponent value (n) acquired from Korsmeyer-Peppas model[27,29].

Statistical analysis:

All the experiments were performed in triplicate and results were expressed as mean±SEM (n=3). The experimental design analysis was implemented by Design-Expert software. All other data were statistically analyzed using GraphPad Prism version 6.01 (SanDiego, CA). Data were analyzed by analysis of variance Bonferroni post hoc test. The p<0.05 was considered statistically significant.

RESULTS AND DISCUSSION

A total 13 formulations of FLS-MS were synthesized in accordance with CCD in order to optimize X1 (drug:polymer) and X2 (surfactant). The t₅₀ (min) (Y1), Q90 (percent) (Y2) and drug content (percent) (Y3). The findings from this research design indicate that drug:polymer (X1) and surfactant (X2) greatly affected FLS-MS. For the quadratic models, the superlative fit for t₅₀ (Y1), Q90 (Y2) and percentage drug content (Y3) was observed owing to its highest r² in contrast to linear, Two Factor Interaction (2-FI) and cubic models[25,30] (Table 2). Hence, the quadratic approach was developed to identify the effects of variables on response parameters as shown:Yᵢ=b₀+b₁X₁+b₂X₂+b₁²X₁²+b₂²X₂²

Fig. 1A, fig. 2A and fig. 3A displayed externally studentized residuals against the predicted values of response variables which showed that the points referring to response variables i.e. Y1, Y2 and Y3 were adjacent to the zero-axis suggesting no consistent bias. Predicted versus actual data graph depicted in fig. 1B, fig. 2B and fig. 3B showed a significant linear curve running through the origin, which confirmed that response parameters were conjunctiva with predicted value[23,24].

The two dimensional (contour) and three dimensional (response surface) plots for Y1-Y3 are presented in fig. 1-fig.3 to illustrate the influence of independent variables on Y1 (t₅₀), Y2 (Q90) and Y3 (percentage drug content). The findings obtained in this study

<table>
<thead>
<tr>
<th>TABLE 2: SUMMARY OF MODEL FIT STUDY FOR RESPONSE PARAMETERS</th>
</tr>
</thead>
<tbody>
<tr>
<td>Models</td>
</tr>
<tr>
<td>Response Y1 (t₅₀)</td>
</tr>
<tr>
<td>Linear</td>
</tr>
<tr>
<td>2-FI</td>
</tr>
<tr>
<td>Quadratic</td>
</tr>
<tr>
<td>Cubic</td>
</tr>
<tr>
<td>Response Y2 (Q90)</td>
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<tr>
<td>Linear</td>
</tr>
<tr>
<td>2-FI</td>
</tr>
<tr>
<td>Quadratic</td>
</tr>
<tr>
<td>Cubic</td>
</tr>
<tr>
<td>Response Y3 (Percentage drug content)</td>
</tr>
<tr>
<td>Linear</td>
</tr>
<tr>
<td>2-FI</td>
</tr>
<tr>
<td>Quadratic</td>
</tr>
<tr>
<td>Cubic</td>
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</tbody>
</table>
Fig. 1: Data analysis of t50% (Y1) (A) externally studentized residual plot; (B) predicted vs. actual plot; (C) contour plot and (D) response surface plot.

Fig. 2: Data analysis of Q90 (Y2) (A) externally studentized residual plot; (B) predicted vs. actual plot; (C) contour plot and (D) response surface plot.
suggested that independent factors influencing $t_{50\%}$ were drug:polymer ($X_1$), surfactant ($X_2$), $X_1^2$ and $X_2^2$ (p<0.05) (Table 3). The quantitative assessment of the important models showed that drug:polymer ($X_1$) and surfactant ($X_2$) had the foremost antagonistic effect on $t_{50\%}$ of FLS-MS, implying that accelerating $X_1$ and $X_2$ values in composition reduces the $t_{50\%}$. This signified that addition of higher amounts of PVP K-30 and Poloxamer 407 to FLS-MS significantly enhances the drug dissolution profile as indicated by decreased $t_{50\%}$ value. The following regression equation represented a fitted model for $t_{50\%}$.

### TABLE 3: ANOVA FOR Y1 ($T_{50\%}$), Y2 (Q90) AND Y3 (% DRUG CONTENT)

<table>
<thead>
<tr>
<th>Source</th>
<th>DF</th>
<th>Sum of squares</th>
<th>Mean square</th>
<th>F-value</th>
<th>p-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Model for Y1</td>
<td>5</td>
<td>118.56</td>
<td>23.71</td>
<td>65.94</td>
<td>&lt;0.0001*</td>
</tr>
<tr>
<td>$X_1$</td>
<td>1</td>
<td>47.48</td>
<td>47.48</td>
<td>132.03</td>
<td>&lt;0.0001*</td>
</tr>
<tr>
<td>$X_2$</td>
<td>1</td>
<td>24.75</td>
<td>24.75</td>
<td>68.82</td>
<td>&lt;0.0001*</td>
</tr>
<tr>
<td>$X_1^2$</td>
<td>1</td>
<td>0.2500</td>
<td>0.2500</td>
<td>0.6952</td>
<td>0.4319</td>
</tr>
<tr>
<td>$X_2^2$</td>
<td>1</td>
<td>9.53</td>
<td>9.53</td>
<td>26.51</td>
<td>0.001*</td>
</tr>
<tr>
<td>Model for Y2</td>
<td>5</td>
<td>475.62</td>
<td>95.12</td>
<td>44.07</td>
<td>&lt;0.0001*</td>
</tr>
<tr>
<td>$X_1$</td>
<td>1</td>
<td>150.84</td>
<td>150.84</td>
<td>69.88</td>
<td>&lt;0.0001*</td>
</tr>
<tr>
<td>$X_2$</td>
<td>1</td>
<td>211.70</td>
<td>211.70</td>
<td>98.08</td>
<td>&lt;0.0001*</td>
</tr>
<tr>
<td>$X_1^2$</td>
<td>1</td>
<td>6.10</td>
<td>6.10</td>
<td>2.83</td>
<td>0.1366</td>
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<tr>
<td>$X_2^2$</td>
<td>1</td>
<td>43.46</td>
<td>43.46</td>
<td>20.13</td>
<td>0.0028*</td>
</tr>
<tr>
<td>Model for Y3</td>
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<td>939.92</td>
<td>187.98</td>
<td>35.75</td>
<td>&lt;0.0001*</td>
</tr>
<tr>
<td>$X_1$</td>
<td>1</td>
<td>684.70</td>
<td>684.70</td>
<td>130.21</td>
<td>&lt;0.0001*</td>
</tr>
<tr>
<td>$X_2$</td>
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<td>10.39</td>
<td>10.39</td>
<td>1.98</td>
<td>0.2026</td>
</tr>
<tr>
<td>$X_1^2$</td>
<td>1</td>
<td>8.01</td>
<td>8.01</td>
<td>1.52</td>
<td>0.2570</td>
</tr>
<tr>
<td>$X_2^2$</td>
<td>1</td>
<td>234.44</td>
<td>234.44</td>
<td>44.59</td>
<td>0.0003*</td>
</tr>
</tbody>
</table>

Note: *p<0.05
Y1 = 42.6 - 2.44X1 - 1.76X2 + 0.25X1X2 - 1.18X1² - 2.43X2²

The perfect fit design for t_{50%} was quadratic (r²=0.9792) (Table 2). As anticipated, fig. IC and fig. ID showed that t_{50%} of FLS-MS was antagonized by significantly increasing the two factors. The F-values and related p-values for response parameters are summarized in Table 3. A model was considered significant if p<0.05. A negative value in quadratic equation indicates an inverse relationship or antagonistic effect between the factor and the response while a positive value in the regression equation exhibits an effect that favors the optimization due to synergistic effect. A negative sign in quadratic formula implies a negative correlation or antagonistic action whilst the positive value in regression model demonstrates synergistic effect of factors on response variables[31,32]. This might be linked to the fact that PVP K-30 and Poloxamer 407 have solubilizing effect on hydrophobic drug particles due to their characteristics of decreasing surface tension and increasing wettability and dispersibility. Therefore, PVP K-30 and Poloxamer 407 helps to improve the dissolution profile of FLS which decreases the t_{50%} value[12,29].

Following equation can explain the effect of factors levels on Q90:

Y2 = 66.82 + 4.35X1 + 5.15X2 + 1.24X1X2 + 2.51X1² + 3.33X2²

Good correlation among adjusted and predicted value had been shown by r² of 0.9692 (Table 2). Q90 (Y2) was dramatically influenced with X1, X2, X1² and X2² (p<0.05). The positive regression coefficient showed that rise in the drug:polymer (X1) could result in a substantial boost in the percentage of drug release which could be correlated to the PVP K-30 and Poloxamer 407 solubilizing action[12,29]. The Q90 pattern is progressively rising to its highest point (region of plot pointing upwards) (fig. 2C and fig. 2D).

The percentage drug content is an incredibly vital consideration for any formulation. As specified in Table 3, main and quadratic effect of drug:polymer has statistically substantial influence on percentage drug content which could be expressed through following regression equation:

Y3 = 78.01 + 9.27X1 + 1.14X2 + 1.42X1X2 - 5.83X1² - 1.33X2²

With an increase in drug:polymer (X1), there was an increasing trend in the values of percentage drug content that might be due to higher quantity of polymer accessible to hold enormous quantity of drugs[33] (fig. 3C and fig. 3D). Drug:polymer showed significant positive effect on X3 as indicated by the large F-value (130.21) (Table 3) and positive coefficient value (b1=9.27).

Graphical plot shown in fig. 4 was obtained using software optimization process which illustrated that the suggested coded levels for X1 and X2 were 0.496 (actual value: 1:3.496) and 1.102 (actual value: 3.102 %), correspondingly which provides 36.33 min, 79.99 % and 81.589 % theoretical value for t_{50%}, Q90 and Q90.
drug content, respectively. An additional batch of FLS-MS was produced with optimal amount of X1 and X2. The experiential t50%, Q90 and percentage drug content for formulated batch were estimated 32 min, 83.9% and 84.6%, respectively, which concurred intimately with the theoretical values[13].

The FTIR spectrum of pure FLS displayed characteristic peaks at 3182, 1602, 1400, 1074, 918, and 882 cm⁻¹ corresponding to O-H stretch (s) of alcohol, C=O (s), aromatic C=C bending (b), C-F (s), =C-H (b) of alkene and aromatic C-H (b), respectively. PVP K-30 spectrum gives peaks at 2971, 1343, 1145, 1670 and 842 cm⁻¹ related to C-H (s), C-H (b), C-N (s), C=O (s) and aromatic C-H (b) groups. Poloxamer 407 FTIR spectra showed characteristic peaks at 3209, 1400, 1110 and 1073 cm⁻¹ comparable to alcohol O-H (s), C-H (b), C-O-C (s) and alcohol C-O (s). Important functional groups peaks of drug and polymers remained intact in spectra of physical mixture. The FTIR spectra of optimized FLS-MS revealed neither appearance of extra peaks nor disappearance of essential distinctive peaks of FLS which established incorporation of drug in microspheres formulation[9,12] (fig. 5).

The PXRD pattern of FLS, PVP K-30, Poloxamer 407, PM and optimized FLS-MS are shown in fig. 6. The abundant diffraction peaks of FLS were observed at 4.67, 6.08, 9.15, 10.27, 11.85, 13.75, 14.71, 16.92, 17.37, 18.84, 19.93, 20.51, 21.24, 22.66, 23.49, 24.82, 25.22, 26.03, 27.58, 28.24, 29.56, 30.53, 31.53, 32.43, 33.23, 34.4, 35.03, 36.7, 38.72, 39.65, 40.86, 41.79, 42.98, 44.01, 45.44, 47.28, 48.24, and 49.17 at 2θ scale which indicated extremely crystalline nature of drug. The absence of peaks in PXRD of PVP K-30 revealed its enormously amorphous characteristics. PXRD of Poloxamer 407 illustrated various peaks at 19.17, 22.69, 23.35, 26.19, 30.8, 32.72, 35.35, 36.19, 39.64, 43.08 and 45.25 at 2θ scale which suggested its semi-crystalline character. PXRD of PM showed the occurrence of several peaks corresponding to FLS and Poloxamer 407 which established drug-polymers compatibility. The diffraction peaks of FLS nearly disappeared in PXRD patterns of optimized FLS-MS, reflecting drug amorphization that could have been through lyophilization applied during FLS-MS production[9,12].

The mean diameter and PDI of FLS-MS using dynamic light scattering was found 0.78 µm and 0.287, respectively which revealed that produced microspheres have smaller size in micrometric range and superior degree of homogeneity as indicated by small PDI value (fig. 7). The smaller diameter of FLS-MS could be attributable to Poloxamer 407 which lowers surface tension at the particles interfaces and thereby providing a shielding barrier which obstructs microspheres aggregation to synthesize smaller size microspheres having uniform particle size distribution[34].

Fig. 5: Fourier transforms infrared spectra of (A) Fluvastatin sodium; (B) PVP K-30; (C) Poloxamer 407; (D) physical mixture and (E) Fluvastatin sodium microspheres
Fig. 6: Powder x-ray diffraction patterns of (A) Fluvastatin sodium; (B) PVP K-30; (C) Poloxamer 407; (D) physical mixture and (E) Fluvastatin sodium microspheres

Fig. 7: Particle size distribution of Fluvastatin sodium microspheres by dynamic light scattering technique
SEM observed the morphological features of FLS-MS and illustrated spherical shape as well as porous rough exterior morphology of microspheres (fig. 8). The surface of FLS-MS was coarse with homogeneous micropores which could be attributed to hydrophilic nature of PVP K-30 and Poloxamer 407 which leached out during lyophilization process and consequently producing pores over the surface of microspheres. Furthermore, particles do not get agglomerates and appears discretely from one another which could be due to high zeta potential and potent surface charge over particles[35].

It is evident from in vitro dissolution study that 25.43%, 27.54% and 91.2% cumulative drug release (% CDR) were achieved from FLS, PM and FLS-MS within 2 h, respectively which demonstrated 3.58-fold improvement in dissolution of FLS through manufacturing of freeze dried microspheres (*p<0.05) (fig. 9). The correlation coefficients for the zero order, first order, Korsmeyer-Peppas, Higuchi and Hixon-Crowell models for FLS-MS were 0.8788, 0.8005, 0.9645, 0.9493 and 0.8329, respectively. Korsmeyer-Peppas model was discovered to be extremely good (y=0.4833x+0.9866, r²=0.9645). The ‘n’ value was 0.48 (<0.45) which demonstrated that drug release from FLS-MS was through Fickian diffusion[14,36] (fig. 10).

FLS-MS rendered a rapid release of 91.2% and 94.21% of drug within 2 and 6 h, whereas FLS-MS-SRT revealed 93.1% drug release through diffusion over 24 h (fig. 11). The slow drug release from matrix tablet could attributable to swelling tendency of eudragit polymeric matrix. According to the Korsmeyer-Peppas equation, the ‘n’ value of 0.5318 indicated an anomalous (diffusion/erosion controlled) drug release mechanism from FLS-MS-SRT[14-17,37] (fig. 12).

In this study, we utilized a combination of freeze dried microspheres and their Eudragit polymers-based matrix tablet techniques in order to acquire improved...
Fig. 10: *In vitro* drug release kinetic model for optimized FLS-MS (A) zero-order; (B) first-order; (C) Korsmeyer-Peppas; (D) Higuchi and (E) Hixon-Crowell model

Fig. 11: *In vitro* drug release profiles of FLS, optimized FLS-MS and FLS-MS-SRT (optimized FLS-MS sustained release tablet)
dissolution profile and sustained release of Fluvastatin sodium to reduce dosage frequency. Solvent evaporated freeze dried microspheres manufactured using PVP K-30 and Poloxamer 407 exhibited 3.58-fold improvement in dissolution of Fluvastatin sodium in 2 h. Furthermore, sustained release of Fluvastatin sodium over 24 h was achieved through Eudragit RL 100 and Eudragit RS 100 based sustained release matrix tablet. The drug release mechanism from FLS-MS-SRT was found anomalous (n=0.5318) which suggested diffusion- along with erosion-controlled release mechanism. Conclusively, it has been shown that the innovative integration of freeze dried microspheres and their Eudragit polymer-based matrix tablet strategies could gain significant

Fig. 12: *In vitro* drug release kinetic model for FLS-MS-SRT (A) zero order; (B) first order; (C) Korsmeyer Peppas; (D) Higuchi and (E) Hixon-Crowell model
potential to boost drug dissolution and sustained release of water-insoluble drugs together with reduced dosage frequency.

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Conflict of interests:

The authors declare that they have no competing interest.

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