

# Disposition and Biocompatibility of Dextrin-coated Cadmium Sulphide Nanoparticles after a Single Dose and Multiple Doses in Rats

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## González *et al.*: Disposition and Biocompatibility of Dextrin-coated Cadmium Sulphide Nanoparticles

To investigate nanoparticles disposition and elimination, dextrin-coated cadmium sulphide nanoparticles were administered intraperitoneally as a single or multiple doses to rats. Nanoparticles distribution in liver, kidney, heart, lung, muscle, testis, brain, spleen and thymus was investigated up to 90 d after daily administration for 30, 60 and 90 d. Tissue distribution was measured in homogenates as fluorescence intensity by spectrophotometry. Tissue concentrations with time for dextrin-coated cadmium sulphide nanoparticles were plotted and some pharmacokinetics parameters were obtained. Serum biochemical parameters were determined using spectrophotometry. Nanoparticles in tissue samples were visualised under an epifluorescence microscope and histological analysis was also performed. After a single administration in rats, nanoparticles were distributed quickly with a  $C_{max}$  occurring in the first 72 hours in all tissues analysed. The elimination  $t_{1/2}$  of nanoparticles was less than 12 days in kidney, spleen, lung and brain; however, it was more than 40 days in muscle, liver and testicle with a mean residence time greater than 50 days. Alterations in glucose, triglycerides and alkaline phosphatase, were observed since the first day and continued throughout the 90 days post dose. Biocompatibility study showed that dextrin-coated cadmium sulphide nanoparticles only produced degenerative alterations in testis and chronic inflammation in lungs after continuous administration during the 90 days. In conclusion, dextrin-coated cadmium sulphide nanoparticles are widely distributed in tissues and have a very long residence time without producing significant toxicity. The multi-dose study showed that these produce selective toxicity after administration for long periods of time. These characteristics make the dextrin-coated cadmium sulphide nanoparticles ideal for theranostic purposes.

**Key words:** Disposition, biocompatibility, nanoparticles, pharmacokinetic

The development of nanomaterials has increased dramatically during the past decade<sup>[1]</sup>. However, currently only very few studies focus on the disposition of nanomaterials *in vivo* as well as the time taken to completely eliminate them in the organisms<sup>[2,3]</sup>. Researchers intended to study nanomaterial biocompatibility need to understand what happens to these after administered to living organisms. Predicting disposition of a nanomaterial is very important in the process of developing new nanomaterials for theranostic use in human beings<sup>[4]</sup>. All preclinical studies on nanomaterials should require a pharmacokinetic study in order to predict and understand the disposition once the nanomaterial enters the organism, when it is finally completely eliminated, and how safe its use is overall. The fate and disposition

of any nanomaterial should be based on its properties, site of administration, formulation, and dosage<sup>[5]</sup>. For this reason, it is necessary to explore biocompatibility, tolerance and characterize the pharmacokinetic profile of each synthesized nanomaterial.

An important parameter to consider in pharmacokinetic studies is the estimated mean time a drug resides in the body within specific tissues; the mean residence time (MRT) can help assess the extent of its efficacy and

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Accepted 05 August 2019

Revised 14 May 2019

Received 11 January 2019

Indian J Pharm Sci 2019;81(5):876-884

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tolerability<sup>[6]</sup>. For nanomaterials, this parameter is also quite essential because the residence time specifies how long it stays in the organism and the estimated time period during which it might identify a pathogenic microorganism, tumor cells or molecular markers for diagnostic purposes, as well as for delivering drugs or genes in therapeutic treatments. Several studies have demonstrated that nanomaterials are delivered to several organs and that these even cross biological barriers<sup>[7-10]</sup>. In addition to this, these have selectivity for specific tissues and remain within for long periods of time, which are ideal properties if they are used to carry drugs, antibodies or vaccines. Few studies reported analysis of nanoparticle disposition and how long these remained inside the tissues before completely eliminated after a single dose administration<sup>[11]</sup>.

These past few years, our group has synthesized and carried out *in vitro* and *in vivo* studies of cadmium sulphide nanoparticles coated with sugar polymers, and found that these were biocompatible and well tolerated in rodents<sup>[12,13]</sup>. Our *in vitro* studies showed dextrin-coated cadmium sulphide (CS-DX) nanoparticles were efficiently delivered at the cellular and subcellular levels<sup>[14]</sup>; additional studies have confirmed effective tissue distribution and safety in rodents after multiple administrations over a short period of time. Given the great tolerability observed in previous studies using experimental animals, those findings suggested that nanoparticles would be rapidly eliminated without producing any biochemical alterations.

The characteristics that have been shown to have the CS-DX nanoparticles suggest that they have the potential to be used for imaging for research and clinical purposes. However, in order to use them with this last purpose it is necessary to know their disposition and their elimination time and also to identify their side effects after multiple doses. Therefore, the present study had two goals. First goal was to characterize CS-DX nanoparticles' disposition after a single dose administered to rats and detailed analysis of a series of pharmacokinetic parameters, such as the  $C_{max}$ ,  $T_{max}$ ,  $AUC_{0-t}$ ,  $AUC_{0-\infty}$ ,  $K_e$  and MRT, along with biochemical parameters while nanoparticles remained in the rats. Rats were observed for a period of 90 d after a single dose administration in order to investigate when these were completely eliminated. The second goal was to address the biocompatibility of CS-DX nanoparticles after daily administration for 30, 60 and 90 d. Biochemical parameters and morphology of certain tissues were studied.

## MATERIAL AND METHODS

All chemicals for the preparation of nanomaterial were purchased from Sigma-Aldrich unless otherwise stated. Commercial diagnostic kits to estimate alanine aminotransferase (ALT), aspartate aminotransferase (AST), alkaline phosphatase (ALP), glucose, cholesterol and triglycerides (TG), urea, creatinine and uric acid were purchased from ELITech, Mexico. Male Wistar rats weighing 110-130 g were obtained by Envigo S.A. (Mexico). All rats were kept in a controlled environment and allowed food (Standard Purina Chow Diet, Mexico) and water *ad libitum*. The rats were fasted for 12 h prior to treatment. Experimental protocols were designed in accordance with the International Guides for practice in animals<sup>[15]</sup>.

### CS-DX nanoparticles:

Cadmium sulphide nanoparticles using dextrin as a capping agent was prepared according to the process described previously<sup>[13]</sup>. Briefly, cadmium sulphide nanoparticles were prepared in aqueous solution. 0.02 M  $CdCl_2$ , 0.5 M KOH, 0.5 M  $NH_4NO_3$ , and 0.2 M  $CS(NH_2)_2$  were added and the mixture was stirred and heated at 80°. Similar conditions were applied to dextrin with 3 % concentration at pH 11. The solution immediately turned a light yellow color, indicating the initial formation of a CS nanoparticle. The temperature of the mixture was kept at 75° and maintained at this temperature for 60 min. The nanoparticles were separated by centrifugation at 6000 rpm during 60 min, and deposited in solid form from the solution; finally, they were washed several times with deionized water and dried at 40° for 24 h.

### CS-DX nanoparticle disposition analysis:

Rats were randomly divided into two groups, control group (n=5) animals were treated with a single ip dose of phosphate buffered saline (PBS, 200  $\mu$ l) and the CS-DX nanoparticle group (n=65) was treated with a single ip dose of 100  $\mu$ g/kg CS-DX nanoparticles prepared in 200  $\mu$ l of PBS. Animals were sacrificed 3, 6, 12, 18, 24, 48, 72, 150, 300, 600, 960, 1440 and 2160 h (90 d) after administration. Five animals were used per time point. A post-mortem macroscopic examination was carried out to search for macroscopic alterations. Tissues were collected and preserved in 10 % neutral-buffered formalin fixative after time samples were processed for a histopathological inspection. Serum samples were also obtained and maintained at -75° for biochemical analysis. Nanoparticle disposition and pharmacokinetic

analysis employed fluorescence quantitative analysis. Liver, kidney, lung, heart, striated muscle, spleen, thymus, brain, and testis were examined. Tissues (50 mg) were homogenized with lysis buffer (20 mM HEPES, 2 mM EGTA, 50 mM  $\beta$ -glycerol phosphate, 5 mM sodium fluoride, 50  $\mu$ M DTT, 100 mM PMSF). The fluorescence was quantified by spectrophotometry (Perkin Elmer) using the excitation wavelength of 485 nm.

Tissues were treated as mentioned above, but samples were not stained and tissues were rinsed with 1 mg/ml solution of sodium borohydride as a blocking agent to reduce autofluorescence. To obtain clear images regarding the disposition of nanoparticles, unstained tissue samples were analysed under an epifluorescence microscope. The amount of nanoparticles was estimated by measuring fluorescence intensity by spectrophotometry in tissue homogenates; the intensity of fluorescence was expressed as arbitrary units (AU). Individual tissue concentration-versus actual time curves were built to derive non-compartmental pharmacokinetic parameters. The pharmacokinetic parameters obtained included,  $C_{max}$ ,  $T_{max}$ ,  $AUC_{0-t}$ ,  $AUC_{0-\infty}$ ,  $T_{1/2}$ ,  $K_e$  and MRT, according to the next Eqns.<sup>[16,17]</sup>,  $K_e = -(\ln C_1 - \ln C_0)/t$ ;  $AUC_{0-t} = AUC_0^t = C_0 + C_1/2(t_1 - t_0) + C_1 + C_2/2(t_2 - t_1) + \dots + C_{n-1} + C_n/2(t_n - t_{n-1})K$ ;  $AUC_0^\infty = C_1/K_e$ ;  $MRT = AUMC_0^\infty/AUC_0^\infty$ .

Maximal concentration ( $C_{max}$ ) was considered as maximal concentration achieved by CS-DX. Time of maximum concentration ( $T_{max}$ ) was considered as the time at which  $C_{max}$  was achieved by CS-DX nanoparticles. The analysis of biochemical parameters was performed using colorimetric methods. The study included glucose, triglyceride, cholesterol, AST, ALT, PA, urea, creatinine and uric acid level quantitation using commercial kits and following manufacturer protocols.

### Biocompatibility of CS-DX nanoparticles in rats:

Twenty four male Wistar rats weighing 110-130 g were assigned to one of four groups: (1) control group rats (6 animals) were treated daily with an ip dose of PBS (200  $\mu$ l) for 90 d; (2) the CS-DX nanoparticle group (18 animals) was treated daily with an ip dose of 100  $\mu$ g/kg CS-DX nanoparticles during 30, 60 or 90 d. After said periods, the animals were sacrificed as described. Tissue samples were processed and observed under a light as well as epifluorescence microscope to carry out a histopathological analysis. A biochemical analysis of blood samples was also performed.

### Statistical analysis:

The data were expressed as the mean $\pm$ SD and statistically analysed using the t-test, and ANOVA calculated with the help of the SPSS 10.0 software (SPSS Inc., Chicago, Ill., USA). Differences were considered significant at  $p < 0.05$ .

## RESULTS AND DISCUSSION

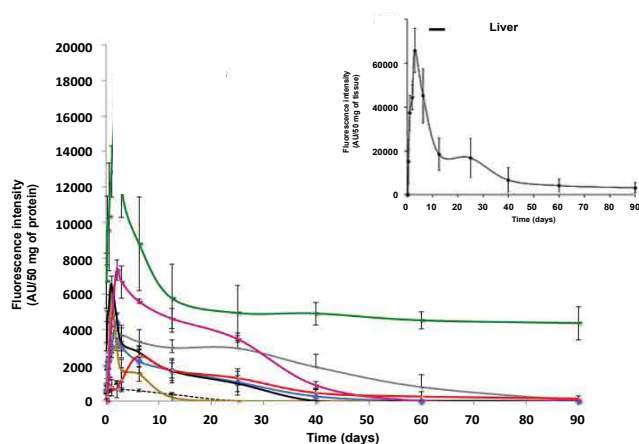
During the study, rodents were closely monitored to ensure they did not suffer side effects from the nanoparticles. Safety assessments consisted of daily observations, body weight and food consumption. A rigorous evaluation was made in order to find out alterations in, motor apparatus (ataxia, tremors, arching, rolling, tonic extension or clonic seizures), central nervous system (anaesthesia, sedation, depression or hypnosis), and physical aspect (lacrimation, exophthalmos, piloerection, salivation or diarrhoea).

Fig. 1 shows the disposition of nanoparticles seen as concentration-time profile and measured as fluorescence intensity (AU) in liver, kidney, heart, lung, spleen, thymus, muscle, brain and testis. The  $T_{max}$ , or observed time to reach the maximum nanoparticle concentration in tissues ( $C_{max}$ ) was mostly between d 1 and 2 (24-48 h), although it remained in muscle at 6.25 d (150 h). The profile curve and pharmacokinetic parameters were different for each tissue studied. The  $C_{max}$  was more intense in liver (65,739 AU) and, consequently, both  $AUC_{0-t}$  and  $AUC_{0-\infty}$  were higher here than in the other tissues (Table 1), reaching  $T_{max}$  on d 3 (72 h). Nanoparticle levels remained high in liver for 40 d, gradually decreasing; however, at 90 d, significant levels of fluorescence were still detected. Interestingly, the calculated MRT for liver was of 69 d with a  $t_{1/2} = 48$  d (elimination half time). The concentration-time profile in lung, kidney, heart, spleen, muscle and thymus was low compared with liver, particularly in thymus ( $C_{max}$  7339, 6018, 3679, 4386, 2515 and 573 AUs, respectively). MRT was different for each tissue: kidney 9.3 d; heart 16 d; lung 14.8 d; spleen 10.4 d, and muscle 59 d. The  $t_{1/2}$  was below 12 d in kidney, heart, lung, and spleen (fig. 1 and Table 1); the muscle had an elongated  $t_{1/2}$  (41.3 d). Interestingly, we also found nanoparticles in brain and testis. The intensity of fluorescence was low in the brain (6561), with a  $MRT=8.5$  d and a  $t_{1/2}=5.9$  d. However, fluorescence intensity was very high in testis (16,810 AUs), with a  $MRT = 83.3$  d and  $t_{1/2} = 58$  d. Fig. 2 shows a representative slice from tissues analysed under light and epifluorescence microscope in stained and non-

**TABLE 1: PHARMACOKINETIC PARAMETERS OF CS-DX NANOPARTICLES AFTER A SINGLE DOSE**

Tissue	C <sub>max</sub> (AU)	T <sub>max</sub> (h)	AUC <sub>0-t</sub> (AU *h)	MRT (d)	T <sub>1/2</sub> (d)	K <sub>e</sub> (h <sup>-1</sup> )
Liver	65 739±1621	72	26 484 058±74650	69±8	48±6	0.0006±0.00008
Kidney	6018±1257	24	519 582±8348	9.3±9	6.41±0.8	0.0045±0.0009
Heart	3679±552	72	3 637 750±45 823	16.0±7	11.1±3	0.0026±0.0007
Lung	7339±2070	48	3 794 373±72859	14.8±6	10.31±4	0.0028±0.0006
Spleen	4386±468	48	1 147 335±93 856	10.4±7	7.04±2	0.0041±0.0009
Brain	6561±1427	24	1 487 975±69784	8.5±4	5.9±0.8	0.0049±0.0005
Testis	16 810±5426	48	11 677 942±79 385	83.3±3	58±12	0.0005±0.00001
Muscle	2515±896	150	1 582 380±99 563	59±8	41.3±17	0.0007±0.00002

Each value represents the average±SD, n=5



**Fig. 1: Single dose time-concentration profiles of CS-DX nanoparticles in tissues in rats**

**Time-concentration profiles of distribution of CS-DX nanoparticles in tissues over a period of 90 d after a single intraperitoneal administration to rats. Each point represents the mean±SD of 5 animals. (—◆—) Spleen, (---) thymus, (—) kidney, (—) heart, (—) brain, (—) testis, (—) lung, (—) muscle**

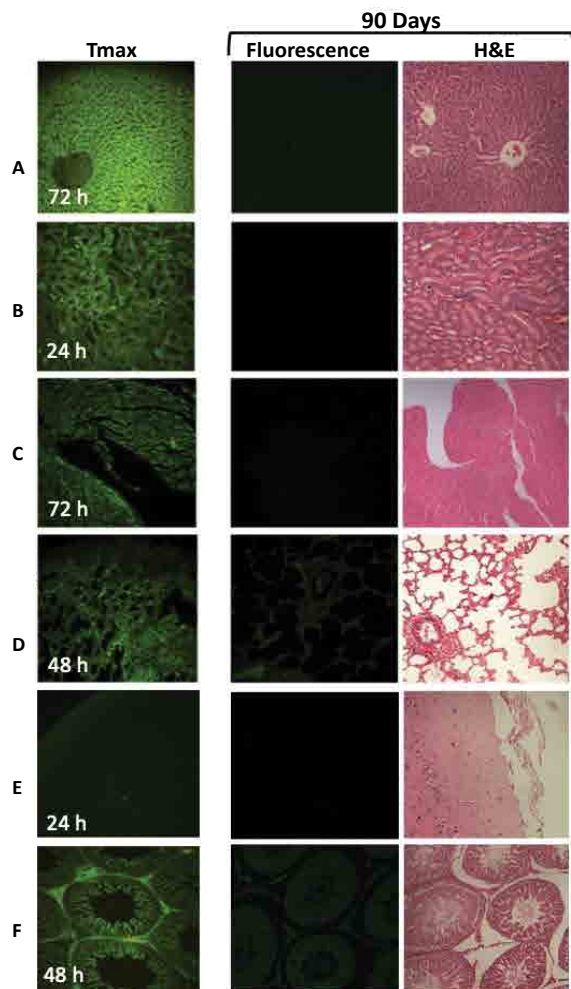
stained samples, respectively; microphotographs were taken during the maximum fluorescence time ( $t_{max}$ ) and at 90 d. CS-DX nanoparticles were identifiable because they emitted green colored fluorescence (fig. 2). The fluorescence intensity was different for each tissue. The histopathological analysis revealed morphological alterations in testis due to the presence of nanoparticles. The changes were characterized by a reduction of Leydig cells, changes in interstitial tissue and seminiferous ducts.

The biochemical analysis showed that CS-DX nanoparticles induced changes in almost all analysed parameters. Fig. 3 shows the variations observed throughout the 90 d of the study, glucose, TG and ALP had important variations. Changes were observed since the first hour until 45 d. However, glucose and ALP subsequently reached normal values by the end of the study (90 d). Triglyceride levels, on the other hand, remained high at 90 d. Slight changes were found in

AST, ALT and urea. No changes were observed in cholesterol, uric acid and creatinine.

Fig. 4 shows representative tissue slices obtained from rats treated daily during 30, 60 and 90 d captured under an epifluorescence microscope. All time periods resulted in a homogeneous distribution of nanoparticles in all analysed tissues. The intensity of fluorescence increased as the treatment time increased. Fig. 5 shows representative slices from tissue stained with H and E. Images from liver, kidney, and brain did not show any morphological alterations, and tissues are quite similar to control. However, microphotographs from the lung region evidenced the presence of an inflammatory infiltrate after 90 d of treatment; on the other hand, testis showed atrophy and degenerative changes 90 d after receiving the CS-DX nanoparticles. Table 2 shows the quantification of biochemical parameters at 30, 60 and 90 d. No alterations were found in rats treated daily with CS-DX nanoparticles for 30 d. Animals treated daily with CS-DX nanoparticles for 60 d showed elevated AP (73 %) and urea (41 %) levels when compared to the control group ( $p < 0.05$ ). However, only urea levels remained elevated (28 %) after 90 d of treatment. No changes were observed in either cholesterol or creatinine levels during all time periods.

In pharmacology, disposition indicates the fate of a drug inside the body, it represents the sum of all absorption, distribution, metabolism and excretion (ADME) processes<sup>[18]</sup>. Although nanomaterials are not drugs, these must nevertheless pass through the same ADME processes once administered to the organism. But it could be assumed these processes are more complex given the physical, chemical and optical properties of nanomaterials. MRT on the other hand<sup>[6]</sup>, help understand the effect span for direct-acting molecules. In the case of nanomaterials, the average time nanoparticles reside in the organism or the average time in which they leave it.

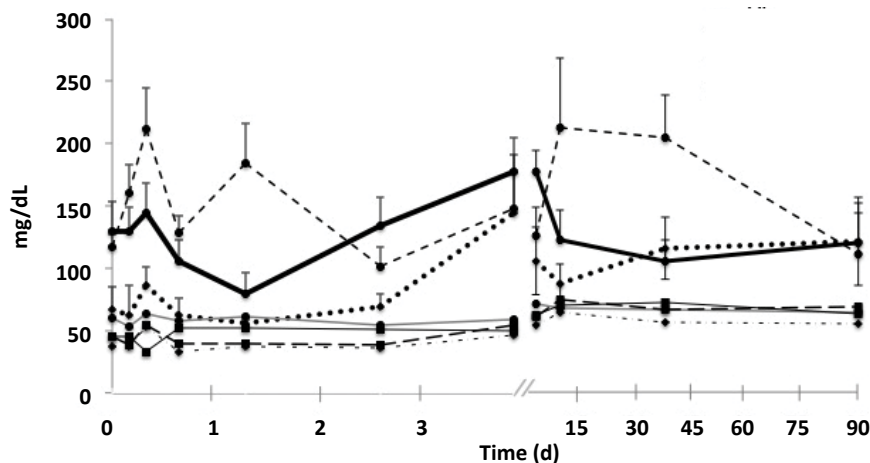


**Fig. 2: Photomicrographs of distribution and localization of CS-DX nanoparticles in rat tissues**

Distribution and localization of CS-DX nanoparticles in tissues from rats treated with a single dose of 100 µg/kg was studied using fluorescence microscopy images that showed the presence of nanoparticles through emission of green color. These images are from A. liver, B. kidney, C. heart, D. lung, E. brain and F. testis at the time of maximal concentration ( $T_{max}$ ) and at 90 d. All tissues were stained with H and E. Magnification 20X

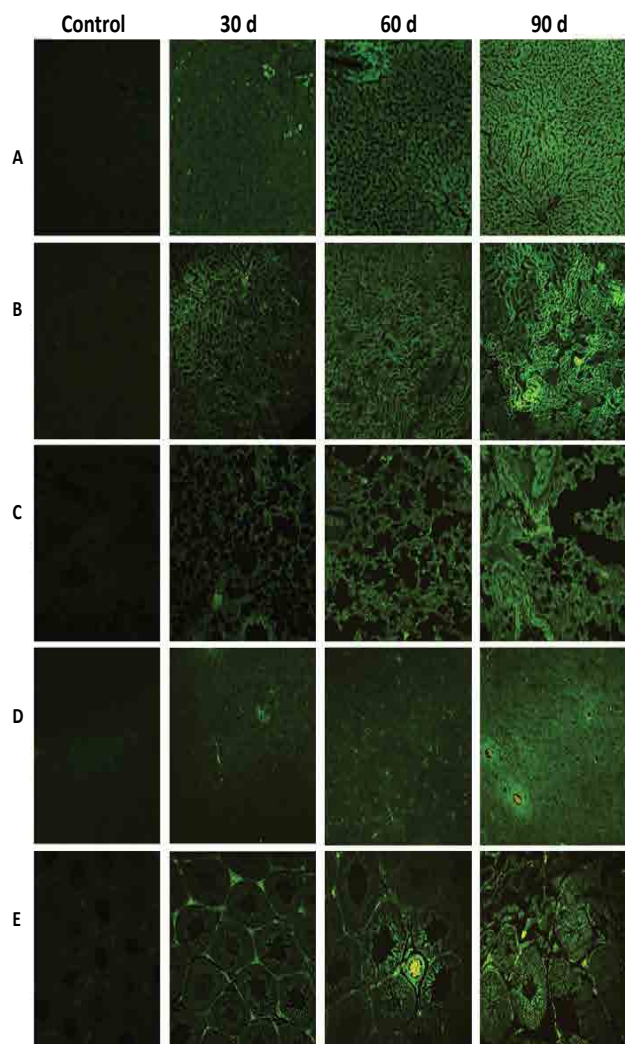
The present study assessed the disposition and biocompatibility of CS-DX nanoparticles administered as a single and multiple doses, respectively. There are currently very few reports on disposition and pharmacokinetics of nanomaterials. Given their size and reduced amounts in blood, this is sometimes easier to quantify in tissues<sup>[19,20]</sup>. Some researchers have developed theoretical models and that their presence in the brain and testicles confirmed that these can cross barriers. Traces of nanomaterials have been detected in long-term studies after administering a single dose without producing toxicity. Cr<sup>3+</sup>-doped zinc gallate,  $Zn_{1.1}Ga_{1.8}Sn_{0.1}O_4:Cr^{3+}$  (ZGO) was administered intravenously over a period of 60 d and no toxicity was observed<sup>[21]</sup>. Orally administered heparin-conjugated deoxycholic acid conjugates also showed no alterations in histology after 45 d<sup>[22]</sup>. Nanomaterial presence in some tissues has also been previously reported, including traces of iron-doped silica nanoshells in lung and liver after 10 w of their administration<sup>[23]</sup>. Carboxylated and pegylated few-layer graphene sheets were found within liver and spleen after 3 mo without producing toxicity<sup>[24]</sup>. These studies and the present study indicate nanomaterials have the capacity to remain for a long period of time in the organism without necessarily producing toxicity. This may be due to their inherent properties.

Modifications in glucose, triglyceride and ALP levels throughout the study were detected, suggesting possible liver damage. Most studies have focused on quantifying nanoparticle levels or identifying their distribution in tissues, while few have analysed their effects on physiological functions. One would expect that, lacking morphological alterations, the tissues



**Fig. 3: Time-biochemical parameter profile after a dose of CS-DX**

Time-biochemical parameter profiles after an intraperitoneal 100 µg/kg dose of CS-DX. Each point represents the mean±SD of 5 animals. (—) Glucose, (· · ·) triglycerides, (—) cholesterol, (— · —) AP, (—) AST, (— · —) ALT, (— · —) urea



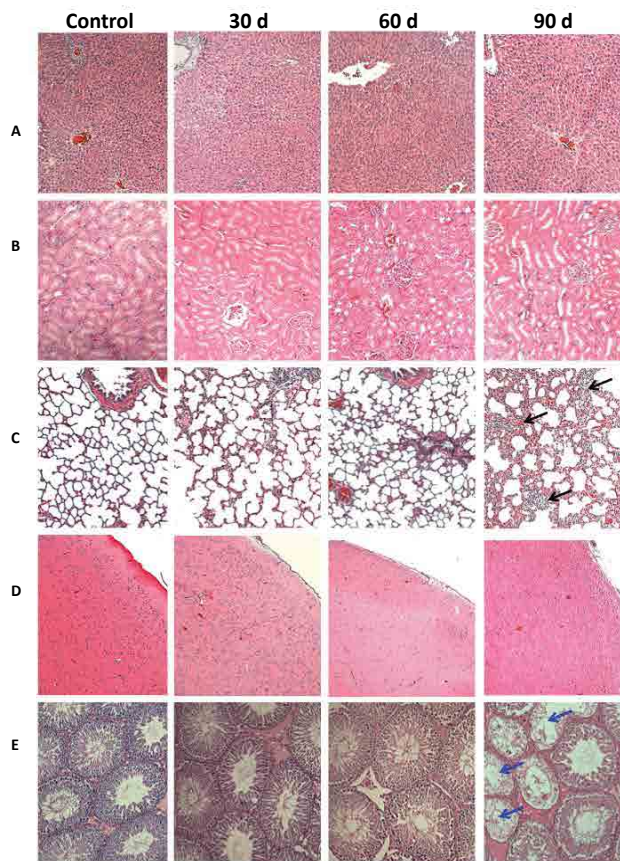
**Fig 4: Photomicrographs of rat tissue sections with distribution and localization of CS-DX nanoparticles**

Animals were treated daily with a dose of 100 µg/kg for 30, 60 and 90 d. Variations in the intensity of green fluorescence in each tissue are evident. Magnification 20X. (A) Liver, (B) kidney, (C) lung, (D) brain, (E) testis

would be functional. While the present study detected variations in biochemical parameters within the initial 24 h, it would seem that, after a long period of time, organs tend to adapt to the presence of nanomaterials and recover their functionality, an hypothesis confirmed by our biocompatibility studies.

Subchronic and chronic treatment with CS-DX nanoparticles demonstrated that these nanomaterials were well-tolerated. No functional or histological alterations were found in tissues from rats administered daily doses during 30 d. At 60 d, no morphological alterations could be seen in any analysed tissues even though there was an increase in ALP and urea levels, suggesting functional alterations in liver and kidney. There was significant toxicity data in animals treated daily for 90 d, which showed degenerative changes in

the testis and inflammation in lungs. Additionally, urea levels remained elevated at this time. Previous studies reported have shown that CS nanoparticles coated with polymers are able to cross biological barriers such as the hemato-encephalic and hemato-testicular ones<sup>[12,13]</sup>. Histologically speaking and given the observations made on rats, it seems the brain is not sensitive to these nanomaterials. However, the testicles appeared to be a particularly sensitive organ to toxic agents and drugs as well as nanomaterials. Nanomaterial toxic effects to testicular cells have been reported. Bara and Kaul reported that ZnO nanoparticles affected steroidogenesis and provoked alterations in phagosomes and lysosomes in Leydig cells<sup>[25]</sup>. Habas *et al.* found that silver-nanoparticles were able to enter sertoli cells and induce apoptosis and oxidative damage altering molecular pathways associated with that process<sup>[26]</sup>. It has also been reported that mice treated with carbonaceous nanoparticles showed changes in sperm viability, morphology and motility<sup>[27]</sup>. Nanomaterial-induced reproductive toxicity induced



**Fig. 5: Tissue histological sections from rats treated daily with CS-DX for 30, 60 and 90 d**

A chronic inflammatory process in lungs after 90 d of treatment was observed (black arrows). Atrophy and degenerative changes in testis after 90 d were observed (blue arrows). Tissue samples were stained with H and E. Magnification 20X. (A) Liver, (B) kidney, (C) lung, (D) brain, (E) testis

**TABLE 2: EFFECT OF CS-DX NANOPARTICLES ON BIOCHEMICAL PARAMETERS IN RATS TREATED DAILY FOR 30, 60 AND 90 DAYS (n=6)**

Parameter	Control	30 days	60 days	90 days
Glucose	140.2±19.4	120.5±36.1	152.0±43.3	159.9±19.4
Triglycerides	60.8±13.7	112.3±51.7	122.4±34.4	187.0±15.5
Cholesterol	54.9±8.9	59.4±12.9	58.7±3.3	64.9±10.3
ALT	54.3±8.6	54.5±8.9	74.9±25	57.5±9.7
AST	160.2±26	168.3±20.1	146.5±40.9	176.1±29.0
AP	121.6±33.7	156.9±13	210±31.4* <sup>#6</sup>	113.8±23.8
Urea	39.6±8.4	35.8±6.6	55.9±8.3* <sup>#</sup>	50.8±2.0 <sup>#</sup>
Creatinine	0.6±0.1	0.5±0.1	0.4±0.1	0.7±0.04
Uric Acid	5.2±1.8	5.6±1.7	10.6±5.4	10.5±3.4

Each value represents the mean±SD. \*P<0.05 compared with control group; <sup>#</sup>p<0.05 compared with 30 d group; \*\*p<0.05 compared with 60 d group; and <sup>6</sup>p<0.05 compared with 90 d group

by is now a topic of interest for several researchers. Recently, several reports have evidenced nanomaterial toxicity in different reproductive organs<sup>[28-32]</sup>.

Toxicity induced by nanomaterials administered not by airway has been previously reported. Wang *et al.* reported an inflammatory process in the lungs after oral administration of halloysite nanotubes to mice, suggesting nanomaterials might accumulate in the lungs, and induce fibrosis<sup>[33]</sup>. On the other hand, other studies have revealed many histological changes in the lung, cellular infiltration and thrombosis in fetuses following an intravenous injection to pregnant rats<sup>[34]</sup>, follicular atresia in female mice<sup>[35]</sup>, and malformation and injury to different organs<sup>[36]</sup>. These results and others suggest that, regardless of the route of administration, lung tissue captures and retains nanoparticles, thus suffering the concomitant toxic effects.

Although the present study revealed several biochemical alterations during the first hour after the administration of a single dose of CS-DX nanoparticles and some of these remained throughout the 90 d, it is striking that, after the administration of multiple doses, the functionality of the organs showed no deterioration. On the contrary, some of the alterations were reversed. As previously indicated, it seems that, after administration, the organs adapt to the presence of nanoparticles and these remain there without producing toxicity in the tissues.

It has been mentioned that cadmium induces several toxic effects to cells and can affect DNA, RNA and proteins<sup>[37-39]</sup>. Even exposure to cadmium-containing nanoparticles could lead to disturbances in cellular homeostatic mechanisms<sup>[40-42]</sup>. Present results demonstrated that CS-DX nanoparticles did not cause severe damage to rats receiving nanoparticles, nor did they produce death. The findings of this study

suggested that CS nanoparticles protected with dextrin control toxicity related to cadmium leakage.

It was observed that CS-DX nanoparticles have a wide distribution and a very long MRT without producing significant toxicity. The multi-dose study showed these nanoparticles were biocompatible and only produced selective toxicity after administration for very long time periods. Due to the high intensity of fluorescence emitted by the CS-DX nanoparticles, it was possible to clearly visualize the tissue morphology; therefore these have the potential to be used in bioimaging in diagnostic and treatment activities. Although nanoparticles have shown to have selective toxicity further research is needed to ensure nanoparticles are safely and efficiently used in medicine.

### Acknowledgements:

The authors would like to thank to Mariana Ortega for her technical assistance. Gerardo González wishes thank CONACYT under grant 254414.

### Conflict of interest:

The author's report no declaration of interest, financial or otherwise regarding this project.

### REFERENCES

1. Thiruvengadam M, Rajakumar G, Chung IM. Nanotechnology: current uses and future applications in the food industry. 3 Biotech 2018;8(1):74.
2. Fennell TR, Mortensen NP, Black SR, Snyder RW, Levine KE, Poitras E, *et al.* Disposition of intravenously or orally administered silver nanoparticles in pregnant rats and the effect on the biochemical profile in urine. J Appl Toxicol 2017;37(5):530-44.
3. Lin X, Gao R, Zhang Y, Qi N, Zhang Y, Zhang K, *et al.* Lipid nanoparticles for chemotherapeutic applications: strategies to improve anticancer efficacy. Expert Opin Drug Deliv 2012;9(7):767-81.
4. Liang X, Wang H, Grice JE, Li L, Liu X, Xu ZP, *et*

- al. Physiologically Based Pharmacokinetic Model for Long-Circulating Inorganic Nanoparticles. *Nano Lett* 2016;16(2):939-45.
5. Yoshikawa T, Nabeshi H, Yoshioka Y. Evaluation of biological influence of nano-materials using toxicokinetic and toxicoproteomic approach. *Yakugaku Zasshi* 2008;128(12):1715-25.
  6. Ďurišová MA. Physiological view and structures of mean residence times. *Gen Physiol Biophys* 2014;33:75-80.
  7. Kettiger H, Schipanski A, Wick P, Huwyler J. Engineered nanomaterial uptake and tissue distribution: from cell to organism. *Int J Nanomedicine* 2013;8:3255-6.
  8. Hara E, Makino A, Kurihara K, Yamamoto F, Ozeki E, Kimura S. Pharmacokinetic change of nanoparticulate formulation "Lactosome" on multiple administrations. *Int Immunopharmacol* 2012;14(3):261-6.
  9. Kaminskas LM, Boyd BJ, Porter CJ. Dendrimer pharmacokinetics: the effect of size, structure and surface characteristics on ADME properties. *Nanomedicine* 2011;6(6):1063-84.
  10. Song X, Zhao X, Zhou Y, Li S, Ma Q. Pharmacokinetics and disposition of various drug loaded biodegradable poly(lactide-co-glycolide) (PLGA) nanoparticles. *Curr Drug Metab* 2010;11(10):859-69.
  11. Qi J, Lu Y, Wu W. Absorption, disposition and pharmacokinetics of solid lipid nanoparticles. *Curr Drug Metab* 2012;13(4):418-28.
  12. Rodríguez-Fragoso P, Reyes-Esparza J, León-Buitimea A, Rodríguez-Fragoso L. Synthesis, characterization and toxicological evaluation of maltodextrin capped cadmium sulfide nanoparticles in human cell lines and chicken embryos. *J Nanobiotechnology* 2012;10:47:1-11.
  13. Reyes-Esparza J, Martínez-Mena A, Gutiérrez-Sancha I, Rodríguez-Fragoso P, González de la Cruz G, Mondragón R, *et al.* Synthesis, characterization and biocompatibility of cadmium sulfide nanoparticles capped with dextrin for *in vivo* and *in vitro* imaging application. *J Nanobiotechnology* 2015;13:2-14.
  14. Gómez-Cansino R, Reyes-Esparza JA, Rodríguez-Fragoso P, González de la Cruz G, Rodríguez-Fragoso L. Long Exposure to CdS-Dextrin Nanoparticles Induces an Immunomodulatory and Anti-Inflammatory Effect in Rats. *J Mater Sci Nanotech* 2017;5(1):2-10.
  15. National Research Council (US), Guide for the Care and Use of Laboratory Animals. 8th ed. National Academies Press, Washington (DC), 2011. Available from: <https://grants.nih.gov/grants/olaw/Guide-for-the-care-and-use-of-laboratory-animals.pdf>.
  16. Zheng H. Intravenous infusion. In: Shargel L, Yu ABC, editors. *Applied Biopharmaceutics & Pharmacokinetics*. 1st ed. New York. McGraw-Hill; 2012. p. 245-312.
  17. Jambhekar SS, Breen PJ. *Basic Pharmacokinetics*. Greyslake (IL): Pharmaceutical Press; 2009.
  18. Hacker M, Bachmann K, Messer W. *Pharmacokinetics modeling. Pharmacology principles and practice*. California: Academic Press; 2009.
  19. Choi SJ, Choy JH. Biokinetics of zinc oxide nanoparticles: toxicokinetics, biological fates, and protein interaction. *Int J Nanomedicine* 2014;9(Suppl 2):261-9.
  20. Saitoh Y, Terada N, Saitoh S, Ohno N, Jin T, Ohno S. Histochemical analyses and quantum dot imaging of microvascular blood flow with pulmonary edema in living mouse lungs by "*in vivo* cryotechnique". *Histochem Cell Bio* 2012;137:137-51.
  21. Sun X, Shi J, Fu X, Yang Y, Zhang H. Long term *in vivo* biodistribution and toxicity study of functionalized near-infrared persistent luminescence nanoparticles. *Sci Rep* 2018;8:10595.
  22. Khatun Z, Nurumnabi M, Lee DY, Kim YJ, Byun Y, Cho KJ, *et al.* Optical imaging, biodistribution and toxicity of orally administered quantum dots loaded heparin-deoxycholic acid. *Macromol Res* 2015;23:686-95.
  23. Mendez N, Liberman A, Corbeil J, Barback C, Viveros R, Wang J, *et al.* Assessment of *in vivo* systemic toxicity and biodistribution of iron-doped silica nanoshells. *Nanomedicine* 2017;13(3):933-42.
  24. Sasidharan A, Swaroop S, Koduri CK, Girish C, Chandran P, Panchakarla LS, *et al.* Comparative *in vivo* toxicity, organ biodistribution and immune response of pristine, carboxylated and PEGylated few-layer graphene sheets in Swiss albino mice: a three month study. *Carbon* 2015;95:511-24.
  25. Bara N, Kaul G. Enhanced steroidogenic and altered antioxidant response by ZnO nanoparticles in mouse testis Leydig cells. *Toxicol Ind Health* 2018;34(8):571-88.
  26. Habas K, Brinkworth MH, Anderson D. Silver nanoparticle-mediated cellular responses in isolated primary Sertoli cells *in vitro*. *Food Chem Toxicol* 2018;116(Pt B):182-8.
  27. Skovmand A, Jacobsen Lauvås A, Christensen P, Vogel U, Sørig Hougaard K, Goericke-Pesch S. Pulmonary exposure to carbonaceous nanomaterials and sperm quality. *Part Fibre Toxicol* 2018;15(1):10.
  28. Mao Z, Yao M, Xu B, Ji X, Jiang H, Han X, *et al.* Cytoskeletons of Two Reproductive Germ Cell Lines Respond Differently to Titanium Dioxide Nanoparticles Mediating Vary Reproductive Toxicity. *J Biomed Nanotechnol* 2017;13(4):409-16.
  29. Adebayo OA, Akinloye O, Adaramoye OA. Cerium oxide nanoparticle elicits oxidative stress, endocrine imbalance and lowers sperm characteristics in testes of Balb/c mice. *Andrologia* 2018; 50(3):12920.
  30. Moshari S, Nejati V, Najafi G, Razi M. Insight into curcumin nanomicelle-induced derangements in male reproduction potential: An experimental study. *Andrologia* 2018;50(2):12842.
  31. Miura N, Ohtani K, Hasegawa T, Yoshioka H, Hwang GW. High sensitivity of testicular function to titanium nanoparticles. *J Toxicol Sci* 2017;42(3):359-66.
  32. Almansour M, Jarrar Q, Battah A, Jarrar B. Histomorphometric Alterations Induced in the Testicular Tissues by Variable Sizes of Silver Nanoparticles. *J Reprod Med* 2017;62(5-6):317-23.
  33. Wang X, Gong J, Rong R, Gui Z, Hu T, Xu X. Halloysite Nanotubes-Induced Al Accumulation and Fibrotic Response in Lung of Mice after 30-Day Repeated Oral Administration. *J Agric Food Chem* 2018;66(11):2925-33.
  34. Lee J, Yu WJ, Song J, Sung C, Jeong EJ, Han JS, *et al.* Developmental toxicity of intravenously injected zinc oxide nanoparticles in rats. *Arch Pharm Res* 2016;39(12):1682-92.
  35. Liu J, Yang M, Jing L, Ren L, Wei J, Zhang J, *et al.* Silica nanoparticle exposure inducing granulosa cell apoptosis and follicular atresia in female Balb/c mice. *Environ Sci Pollut Res Int* 2018;25(4):3423-34.
  36. Zhang Y, Wu J, Feng X, Wang R, Chen A, Shao L. Current understanding of the toxicological risk posed to the fetus



- following maternal exposure to nanoparticles. *Expert Opin Drug Metab Toxicol* 2017;13(12):1251-63.
37. Li KG, Chen JT, Bai SS, Wen X, Song SY, Yu Q, *et al.* Intracellular oxidative stress and cadmium ions release induce cytotoxicity of unmodified cadmium sulfide quantum dots. *Toxicol Vitro* 2009;23:1007-13.
  38. Ospondant D, Phuagkhaopong S, Suknuntha K, Sangpairoj K, Kasemsuk T, Srimaroeng C, *et al.* Cadmium induces apoptotic program imbalance and cell cycle inhibitor expression in cultured human astrocytes. *Environ Toxicol Pharmacol* 2019;65:53-9.
  39. Adebambo OA, Shea D, Fry RC. Cadmium disrupts signaling of the hypoxia-inducible (HIF) and transforming growth factor (TGF- $\beta$ ) pathways in placental JEG-3 trophoblast cells via reactive oxygen species. *Toxicol Appl Pharmacol* 2018;342:108-15.
  40. Naderi S, Zare H, Taghavinia N, Irajizad A, Aghaei M, Panjehpour M. Cadmium telluride quantum dots induce apoptosis in human breast cancer cell lines. *Toxicol Ind Health* 2018;34(5):339-52.
  41. Liu J, Hu R, Liu J, Zhang B, Wang Y, Liu X, *et al.* Cytotoxicity assessment of functionalized CdSe, CdTe and InP quantum dots in two human cancer cell models. *Mater Sci Eng C Mater Biol Appl* 2015;57:222-31.
  42. Nan C, Yao H, Yuanyuan S, Xiaoming L, Qing H, Haifeng W, *et al.* The cytotoxicity of cadmium-based quantum dots. *Biomaterials* 2012;33:1238-44.
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