Inhibition of Colon Cancer Cells Proliferation and Invasion by Etoposide Loaded on Nano-Suspensions Containing Black Currant Seed and Evening Primrose Oils

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Formulating etoposide into a nanoemulsion based on combining two natural oils, Ribes nigrum (black currant) seed oil and organic evening primrose oils may improve its antineoplastic activity in cancer cells. The present study aimed to synthesize, characterize and in vitro evaluate the cytotoxic effect of formulating etoposide-loaded (black currant) seed oil and organic evening primrose oils on Colorectal Carcinoma colon cancer cells. The anti-proliferation and anti-invasion effects of the produced formula on Colorectal Carcinoma were investigated by the cell counting kit-8 and the collagen-based cell invasion assay, respectively. Mitochondrial staining kit, annexin Fluorescein isothiocyanate double staining, and nucleosome detection were used to discriminate the stages of apoptosis. According to the dynamic light scattering results, formulating etoposide-loaded (black currant) seed oil consisted of nanodroplets with z-average diameters of 144.6±5.3 nm and mean surface charge of -0.081±0.001 mV. Only (1.7±1.3) µM of formulating etoposide-loaded (black currant) seed oil was able to cause 50 % reduction in the Colorectal Carcinoma cellular growth which was strikingly lower than that of free-formulating etoposide (18.1±2.5 µM) by around ten-fold. The superior apoptotic effect of Formulating etoposide Ribes nigrum (black currant) seed oil and organic evening primrose oils relative to free-formulating etoposide on the Colorectal Carcinoma cells was ascertained by the enhanced mitochondrial depolarization, higher nucleosomal ratio and increased amount of early and late apoptotic cellular populations. The Formulating etoposide Ribes nigrum (black currant) seed oil and organic evening primrose oils treatment impeded the invasion of colorectal carcinoma cells by (54.8±1.2) %, which was greater than the free-formulating etoposide treatment that deterred only (35.1±1.2) % of the invaded cells. In conclusion, the incorporation of formulating etoposide into a nanoemulsion formulated from the bioactive natural oils potentiates its antitumor activity in colon cancer cells.

Key words: Natural oils, polyunsaturated fatty acids, nanocarrier, zetasizer measurement, nucleosomes, apoptosis

According to the statistical report on cancer introduced by GLOBOCAN 2018, colon cancer represents the most common malignant tumors diagnosed worldwide. It ranks the third in terms of incidence while in terms of mortality, colon cancer arises to the second common causes leading to the death following lung cancer[1-3]. In addition to the drug resistance, metastasis is the main obstacle for effective therapies, which could lead to increasing the death rate of colon cancer patients[4-5]. Chemotherapy is one of the possible options available for cancer treatments. In general, continuous exposures to the chemotherapeutic agents for a prolonged period are obliged for effective cancer therapy, which is not feasible for formulating etoposide (ETP) owing to the lower solubility, short biological half-life and bioavailability[6]. Moreover targeting and efficient delivery of the anti-cancer agent at the tumor site, while preventing severe damage is the main hurdle in cancer treatment.
diagnosis and therapy\(^7\). Therefore, it is necessary to propose new deliveries for the chemotherapeutic agents that improve their selectivity at the target site.

Polyunsaturated fatty acids (PUFAs) are one of the most natural oils that possess anti-cancer and anti-microbial activity. The beneficial properties of PUFAs could be ascribed to their safety, high efficacy, a broad range of activity and absence of resistance mechanisms. Furthermore, it could be used as a tumor-specific ligand to guide antineoplastic agents selectively at the tumor site without affecting the other healthy cells\(^8-10\).

Nanoemulsion with the mean of the small droplet size ranging from 20-200 nm is one of the most promising nano-delivery systems. Nanoemulsions are dispersion systems that consist of water and oils, stabilized by emulsifying agents, surfactants and cosurfactants. It has numerous advantages as nanocarrier, which include targeting drug delivery, stability, enhancing the solubility of the hydrophobic drug and providing protection of drugs from degradation\(^11-12\). Although ETP was loaded in many nanoparticles, such as solid lipid carriers and poly (lactide-co-glycolide) nanoparticles, it has never been loaded in PUFAs nanoemulsions\(^13-14\). The present study aimed to incorporate ETP into nanoemulsion based on mixing natural oils, *Ribes nigrum* (black currant) seed oil (BLC) and organic evening primrose oils (EVP) and evaluate its apoptotic and anti-invasion activities on colon cancer cells.

**MATERIALS AND METHODS**

**Materials:**

ETP was purchased from Ebewe Pharma GmbH (Unterach, Austria). Organic evening primrose oil (EVP) and BLC were obtained from Chateau Cosmetics Botanical Beauty (Miami, FL, US). The main component of two oils was linoleic acid, gammalinolenic acid, omega 3, 6 and 9. Tween 80 (T80) and span 20 (S20) were acquired from Sigma (Missouri, US). All the tissue culture supplies were purchased from UFC Biotechnology, Inc. (Riyadh, KSA). The 4',6-diamidino-2-phenylindole DAPI dihydrochloride was acquired from Invitrogen (NY, US). Cell Counting Kit- 8 (CCK-8) (Lot. No. LE612) was procured from Dojindo Molecular Technologies, Inc. (JAPAN). Annexin V-FITC Apoptosis Detection Kit (Cat. No. MBS668896) was obtained from MyBioSource, Inc. (San Diego, CA, US). Mitochondria Staining Kit (Cat. No. CS0390) was acquired from Sigma (CA, US).

**Synthesis of nanoemulsion formulas:**

The nanoemulsion (BLC-EVP-NANO) was produced by the ultrasonication method. In brief, different volume fractions (v/v) of 2 % BLC, 2 % EVP, 7 % T80, 3 % S20 and 86 % sodium acetate buffer (pH 5) were mixed at 25\(^\circ\). Then, the mixture was sonicated for 20 min until it became clear and transparent with the Omni Sonic Ruptor 4000 Ultrasonic Homogenizer (NY, US). The drug-loaded formulation (ETP-BLC-EVP-NANO) was prepared by directly solubilizing the ETP in BLC-EVP-NANO.

**Physical characterization of nanoemulsion formulations:**

The absorption spectra for droplet size distributions of BLC-EVP-NANO and ETP-BLC-EVP-NANO were measured at the wavelength (200-600 nm) using Ultraviolet-visible (UV-Vis) spectrophotometer (Thermo Scientific\(^\text{TM}\), US). The droplet sizes and zeta potentials of the dispersed nanodroplets for BLC-EVP-NANO and ETP-BLC-EVP-NANO were assessed using the Zetasizer (Malvern Instruments Ltd., UK).

**In vitro drug release:**

The dialysis technique evaluated the *in vitro* release of the ETP and ETP-BLC-EVP-NANO. Both formulations (1 ml) were transferred into the dialysis bag separately (Cut-off 3.5 Da, Spectra Lab, CA, US). Then, the bag was incubated into the phosphate buffer (200 ml, pH 7.4) and stirred at 1 g. Nearly, 1 ml of the buffer was taken at a predetermined interval and replaced by fresh buffer (1 ml). The removed buffer absorbance at a specific time (A1) was measured by using a UV-Vis spectrophotometer (Thermo Scientific\(^\text{TM}\), US). The release of ETP (%) was measured by means of dividing A1 by A0 (absorbance of the initial drug sample added to the dialysis bag) and multiplying by 100.

**Assessment of antitumor activity:**

**Cell culture:** The colon cancer cell line (HCT116) was purchased from America Type Tissue Culture Collection (Manassas, VA, USA). The 2×10\(^6\) HCT116 cells were plated in a culture flask (25 cm\(^2\)) containing 5 ml of Dulbecco’s modification of eagle’s medium (DMEM), complemented with 10 % fetal bovine serum (FBS), 1 % penicillin /streptomycin and incubated at 37\(^\circ\) in a 5 % CO\(_2\) humidified atmosphere. For subculture, the DMEM was discarded, cells rinsed with phosphate-buffered saline (PBS) and detached from flasks by adding 1 ml of 0.25 % trypsin. The cells were nourished
with DMEM until 90% confluence was obtained.

**Cell counting kit-8:** The 1×10⁴ of HCT116 cells were cultured into 96-well plate at which each well contained 100 μl of growth medium followed by incubation at 37°C for 24 h in a CO₂ incubator. Then, 200 μl of ETP (0.5-3 μM), BLC-EVP-NANO (0.5-3% v/v) and ETP-BLC-EVP-NANO (0.5-3 μM) were added to each well and incubated at the same culture conditions. In order to evaluate the cellular proliferation, 5 μl of CCK-8 reagent was added in the dark into each well, mixed gently, and incubated for 3 h at culture conditions. After that, the absorbance (A) of treated cells, media containing cells (control) and media (blank) were assessed in a BioTek Microplate Reader (λ= 450 nm). The cellular proliferation (CP %) was calculated by subsequent calculation:

\[ \text{CP} \% = \frac{(A \text{ of treated cells} - A \text{ of blank})}{(A \text{ of control})} \times 100 \]

**Cell morphology characterization:** Cells (1×10⁴/well) were plated at 100 μl of DMEM into a 96-well. Then, 200 μl of the IC₅₀ for ETP, BLC-EVP-NANO, and ETP-BLC-EVP-NANO were added to each well and incubated for 24 h at 37°C. After that, DMEM was removed, cells were rinsed with buffer saline (100 μl), fixed by the addition of formaldehyde (200 μl, 4%), and stained with 100 μl of 5% Coomassie brilliant blue dye (Fisher Scientific, US) for 10 min. Finally, cells were cleaned with tap water followed by drying overnight at 25°C. The morphological alteration of treated cells was detected using a phase-contrast inverted microscope (Olympus, Japan).

**Nuclear DNA Staining:** Cells (5×10⁴/well) were cultured in 500 μl of DMEM in a 24-well plate and incubated for 24 h at 37°C. Then, 500 μl of the IC₅₀ for each tested formulation was added and incubated for 24 h. Following incubation, cells were rinsed with PBS (300 μl), fixed via 4% formaldehyde (200 μl), stained for 2 min with DAPI stain (300 μl, 300 nM) and visualized using fluorescent microscope at 437 μm (Leica CRT6000, Germany).

**Mitochondrial polarization assay:** JC-1, 5,5',6,6'-tetrachloro-1,1',3,3'-tetraethylbenzimidazolylcarboxyanine iodide) is a cytofluorimetric, lipophilic, cationic dye, used to assess the mitochondrial membrane polarization of HCT116 cells. Briefly, cells (1×10⁴/well) were cultured into 100 μl of growth medium into 96 well-plates. Then, 200 μl of IC₅₀ for various treatments were added to each well. After 24 h incubation, cells stained by JC-1 solution (JC-1 stain, JC-1 buffer solution, and DMEM) and incubated for 30 min at 37°C. Finally, the fluorescence was examined at excitation (Ex): 525 nm/emission (Em): 590 for red fluorescence (depolarization) and at Ex:490nm/Em:530 for green fluorescence (hyperpolarization) using fluorescence microplate reader (Synergy™ HTX, BioTek, US).

**Annexin V-FITC/PI assay:** HCT116 cells (3×10⁴/well) were cultured at 2 ml of DMEM into six well-plates and incubated at culture conditions. Then, 2 ml of IC₅₀ for each tested formulation was added to each well. Following 24 h incubation, cells were harvested, rinsed with pre-cold PBS, centrifuged (300 g), re-suspended in 100 μl of 1X binding buffer, and transferred to a flow cytometry tube. Then, 5 μl of each FITC and PI added to the cell suspension, incubated for 20 min and completed with 400 μl of binding buffer. Finally, cells evaluated within one hour using flow cytometer (FACS Aria™ III, BD Biosciences, CA, US).

**Nucleosome assays:** The ratio of nucleosome was analyzed by utilizing Cell death detection ELISA kit (Lot. No. 19315700) (Mannheim, Germany). Briefly, HCT116 cells (1×10⁴/well) were cultured at 100 μl of growth medium in each well of the 96 well-plates and incubated at culture conditions. Then, 200 μl of the IC₅₀ of different formulations was added to each well and incubated for 24 h. Following incubation, the plate was spun down (200 g), and the cells were suspended in the lysis solution. The lysates (20 μl) were transferred to a streptavidin-coated microplate, complemented with 80 μl of immunoreagent, and incubated on a shaker (10 g) at the dark for 2 h. After that, the ABTS stain was added, incubated on a plate shaker for 10 min and stopped by ABTS stop solution. The absorbance (A) was determined at 405 nm. The nucleosome ratio was calculated according to the following equation:

\[ \text{Nucleosome ratio} = \frac{(A \text{ of the treated cell (dead cells)}/ A \text{ of the control cell (viable cells)})}{(A \text{ of control})} \]

**Invasion assay:** The QCM™ 24-well Collagen-based Invasion Assay (Cat.No. ECM551, Merck KGaA Darmstadt, Germany) was used to evaluate the invasion capability of HCT116 cells. Briefly, the 3×10⁴ cells/well were cultured into a 6-well plate containing 2 ml of growth medium. Then, 2 ml of IC₅₀ for each tested formulation was added to each well. After that, media without FBS (300 μl) was supplemented to each insert and incubated at 37°C for 30 min. Then, 250 μl of media were extracted and 250 μl of cells suspension was added
into each insert suspended in 500 µl of the media with 10 % FBS in the lower chamber. Then, the plate was covered and incubated for 24 h in the CO₂ incubator. After that, all non-invaded cells were detached, and the insert was placed in 400 µl of cell stain for 20 min. Then, the insert was rinsed, gently cleaned, transferred into 200 µl of extraction buffer and left for 15 min at 25 °C. Finally, 100 µl of the extracted buffer were shifted to a 96-well culture plate for colorimetric measurement at 560 nm. The HCT116 cell invasion was measured according to the subsequent equation:

Relative Invasion (%) = (A of treatment/A of control) * 100

**Statistical analysis:** One-way ANOVA was used to estimate the statistical analyses between samples. The p-values were measured according to the pairwise t-tests and considered statistically significant when p<0.05. Data were expressed as mean±standard deviations for three determinations (n=3). The statistical analyses were carried out using MegaStat Excel Software (version 10.3, Butler University, Indianapolis).

**RESULTS AND DISCUSSION**

Although the maximum absorptions for each produced formula, BLC-EVP-NANO, and ETP-BLC-EVP-NANO, was recorded at the same wavelength ($\lambda_{max}$=300 nm), the amounts of absorbances for ETP-BLC-EVP-NANO were larger than these of BLC-EVP-NANO at each wavelength (p<0.001, fig. 1). The distribution around the maximum absorption for both formulas was implied by measuring the kurtosis which was 2.3 and 1.1 for the absorption curves of BLC-EVP-NANO and ETP-BLC-EVP-NANO, respectively which indicate that both absorption spectrums were platykurtic and have a broad distribution of the absorbances at different wavelengths.

The z-average diameters, coefficient of variations and zeta potentials for the formulated nanoemulsions, BLC-EVP-NANO and ETP-BLC-EVP-NANO were summarized in Table 1. The nanodroplet sizes and surface charges of BLC-EVP-NANO were considerably changed when loaded with ETP. According to the measured coefficient of variations among the droplets sizes, the small values for both formulas imply normal and homogeneous distribution among the nanodroplets.

According to fig. 2, 35 % of ETP-BLC-EVP-NANO was released at the initial hour compared to 12 % of the native ETP solution. Following the initial hour, a sustained release of both ETP-BLC-EVP-NANO and native ETP was observed. Within six hours, almost 90 % of the ETP-BLC-EVP-NANO and only 50 % of the ETP were released.

The percentages of the proliferative HCT116 cells subjected to the ETP, BLC-EVP-NANO, and ETP-BLC-EVP-NANO at various concentrations (0.5 µM, 1 µM, 1.5 µM and 3 µM) were set out in fig. 3. Interestingly, the proliferation of BLC-EVP-NANO and ETP-BLC-EVP-NANO treated cells were markedly lower than the growth of ETP treated cells at all tested concentrations. The measured half-maximal inhibitory concentration (IC₅₀) for BLC-EVP-NANO (3.1±1.7) µM and ETP-BLC-EVP-NANO (1.7±1.3) µM were strikingly lesser than that of ETP (18.1±2.5) µM (p<0.001).

**Table 1:** The physical characteristics of the nanodroplets for BLC-EVP-NANO and ETP-BLC-EVP-NANO. The (*) referred to the extremely highly significant difference between BLC-EVP-NANO and ETP-BLC-EVP-NANO.

<table>
<thead>
<tr>
<th></th>
<th>BLC-EVP-NANO</th>
<th>ETP-BLC-EVP-NANO</th>
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<tbody>
<tr>
<td>Z-average diameter (nm)</td>
<td>59.42±2.5</td>
<td>144.6±5.3***</td>
</tr>
<tr>
<td>Zeta potential (mV)</td>
<td>-0.183±0.002</td>
<td>-0.0808±0.001***</td>
</tr>
<tr>
<td>Coefficient of variation</td>
<td>0.04 ± 0.01</td>
<td>0.03 ± 0.01</td>
</tr>
</tbody>
</table>

**Fig. 1:** UV-Vis absorption spectra for particle size distributions of BLC-EVP-NANO and ETP-BLC-EVP-NANO

**Fig. 2:** The release of native ETP and ETP-BLC-EVP-NANO in phosphate buffer (pH 7) at 37°C
As shown in fig. 4 (a and b), most of the untreated HCT116 cells (control) displayed a homogenous cell shape, intact cell membrane, and normally rounded nucleus that indicates the cell viabilities. On the other hand, a decrease in cell count, irregular cell shape and membrane blubbing were revealed in cells treated with all formulations. In fact, the signs of late apoptosis, such as nucleus fragmentation and chromatin condensation were higher in cells treated with BLC-EVP-NANO and ETP-BLC-EVP-NANO.

The mitochondrial polarization ratio of HCT116 cells treated with the IC\textsubscript{50} of the various formulations was exhibited in fig. 5. The mitochondrial hyperpolarization (high red fluorescence) was detected in the untreated HCT116 cells (control), which was an indication of the cell viability. In contrast, the mitochondrial depolarization, indicated by the lowered red/green fluorescence intensity ratio, was markedly detected in the cells treated with ETP-BLC-EVP-NANO (\(p<0.001\)).

The apoptotic stages of the untreated and treated HCT116 cells were categorized according to their ability to stain with annexin V-FITC and PI as shown in the flow cytometry plots (fig. 6). The percentages of the treated HCT116 cells differentiated according to the stages of apoptosis were quantified as illustrated in Table 2. The ETP-BLC-EVP-NANO treatment caused a significant enhancement in the amount of late apoptotic cells and lowered the amount of the viable cells when compared to the ETP and BLC-EVP-NANO treatments.

The ratio of nucleosomes in the cytoplasm of the apoptotic HCT116 cells following treatment with the IC\textsubscript{50} of ETP, BLC-EVP-NANO and ETP-BLC-EVP-NANO were clarified in fig. 7. The lowest amount of nucleosomes was markedly detected when cells were treated with ETP. In contrast, the ratio of nucleosomes of the cells treated with BLC-EVP-NANO and ETP-BLC-EVP-NANO were noticeably increased to 6.8±0.09 and 9.7±0.09 respectively, when compared to that of ETP treated cells (4.5±0.06).

The capability of the various formulations to suppress the HCT116 cell invasion was revealed at the microscopy images (fig. 8). The highest inhibition of HCT116 cell invasion was detected with ETP-BLC-EVP-NANO treatment (\(p<0.001\)). BLC-EVP-NANO treatment had also considerably impeded the invasion ability of HCT116 cells when compared to the untreated and ETP treated cells (\(p<0.001\)).

Polyunsaturated fatty acids (PUFAs) as an active agent of natural oils have several properties such as anti-microbial and anti-cancer activity. PUFAs are placed at the front of the biotechnological study owing to the potent activity of these compounds in the pharmacy\cite{9}. Using nanoemulsions in cancer therapy has become more promising owing to their larger surface area, superficial charge, bioavailability, specific targeting and easy accumulation in the cancer cell\cite{15}. In the current study, both BLC and EVP, which are natural oils enriched with PUFA, were formulated with tween.
Table 2: The Percentages of HCT116 Cells Differentiated According to the Stages of Apoptosis

<table>
<thead>
<tr>
<th>Type of cells</th>
<th>Late apoptotic (Q2)</th>
<th>Early apoptotic (Q4)</th>
<th>Necrotic (Q1)</th>
<th>Viable (Q3)</th>
</tr>
</thead>
<tbody>
<tr>
<td>ETP</td>
<td>37.83±0.61</td>
<td>36.36±1.26</td>
<td>5.23±0.37</td>
<td>20.53±1.58</td>
</tr>
<tr>
<td>BLC-EVP-NANO</td>
<td>38.7±3.91</td>
<td>36.5±2.59</td>
<td>4.8±0.61</td>
<td>19.63±1.51</td>
</tr>
<tr>
<td>ETP-BLC-EVP-NANO</td>
<td>42.33±1.72**</td>
<td>38.5±1.27</td>
<td>5.66±1.14</td>
<td>13.46±0.57**</td>
</tr>
</tbody>
</table>

Data were expressed as mean ± SD (n=3). The p-values were assessed using the independent t-tests between the variables. The (**) referred to the highly significant differences (0.001 ≤ p < 0.01) with respect to ETP.

Fig. 6: Annexin V-FITC/PI flow cytometry plots of untreated and treated HCT116 with the IC_{50} of the various formulations

Fig. 7: The ratio of the nucleosome in HCT116 cells subjected to the IC_{50} of ETP, BLC-EVP-NANO, and ETP-BLC-EVP-NANO. Error bars represented the ±SD. The p-values were assessed according to the one-way ANOVA and measuring the pairwise t-tests. The (***and***) referred to the high (p < 0.01) and very highly significant difference (p < 0.001) between ETP and the other tested formulas.

Fig. 8: Light microscopy images of the invasion for the untreated and 24 h -treated HCT116 cells (20X magnification). The percentages of the impeded cells from invasion, subjected to different treatments, are shown below each image.
80 and span 20 in a buffer (pH5) to produce oil-in-water NE with the aim to facilitate the delivery of ETP and improve its antineoplastic effect on the colon cancer cells. The droplet sizes for both produced formulas, BLC-EVP-NANO and ETP-BLC-EVP-NANO, were lower than 150 nm and distributed in a monodisperse pattern. The noticeable increase of droplet size for ETP-BLC-EVP-NANO relative to BLC-EVP-NANO might be evidence that ETP was trapped inside the BLC-EVP-NANO formula. In agreement with our result, a previous study revealed that the incorporated ifosfamide with camphor-NE displayed a larger droplet size than the blank camphor-NE[16]. Likewise, the UV-Vis measurement showed that the absorptions of the BLC-EVP-NANO were obviously increased when loaded with ETP. The previous study on gold nanoparticles carried out by Doak et al.[17] exhibited that the larger particle size was combined with larger absorbance at the long wavelengths. It is worth pointing out that the small and monodisperse size distribution of ETP-BLC-EVP-NANO might be leading to the complete release of ETP-BLC-EVP-NANO subsequently 24 h.

Regarding HCT116 cell proliferation, the IC$_{50}$ of ETP-BLC-EVP-NANO (1.7±1.3) was markedly decreased with around ten-folds than the ETP (18.1±2.5) µM. Narrowest droplet size with a monodisperse distribution of ETP-BLC-EVP-NANO was expected to raise the cellular uptake of the formulation and enhanced its adhesion to the cancer cells[18]. Additionally, the decline in the proliferating of HCT116 cells with ETP-BLC-EVP-NANO treatment could be accredited to the synergistic effect of the natural active agents of oils and ETP. Similarly, our recent study conducted on lung cancer cell line A549 cells showed a decrease in cellular growth when cells treated with etoposide encapsulated nanoemulsion prepared in sodium phosphate buffer (pH 7) compared to the free ETP which has no noteworthy effect on A549 cells[19]. The anti-inflammatory and anti-proliferative effect is one of the most pharmacological effects of EVP oil[20].

The early event of apoptosis in HCT116 cells treated with ETP, BLC-EVP-NANO and ETP-BLC-EVP-NANO was detected in the morphological changes observations using light microscopy. The changes, such as irregular cell shape and membrane blubbing were higher in the treated HCT116 cells. Besides, the mitochondrial depolarization, which was evaluated by lowering the red/green fluorescence intensity ratio was higher with ETP-BLC-EVP-NANO treatments. Along with the mitochondria, the nucleus was the most critical organelles for cell proliferation and apoptosis. Therefore, the main goal of cancer therapy is to target the nucleus that controlled the processes leading to cell apoptosis[21]. Interestingly, the increased percentage of late apoptotic cells with ETP-BLC-EVP-NANO treatments could be an indication that the ETP-BLC-EVP-NANO formula was affecting the DNA. This finding was confirmed with the cell death assay, which showed the maximum amounts of the nucleosomes at the cytoplasm of apoptotic HCT116 cells treated with the ETP-BLC-EVP-NANO. Consequently, loading ETP on natural oil-based nanoemulsions possibly will enhance the induction of apoptosis in cancer cells. Recently, several studies have reported that incorporating chemotherapeutic agents into nanoemulsions based on carrot seed oil, garlic oil, ginger oil and flaxseed oil had potentiated the effectiveness of the chemotherapeutic agent toward cancer cells[22-23-24-25]. The invasion is a critical component in the escape and propagation of tumor cells from the main site into distant organs[26]. In the present study, treatment with ETP-BLC-EVP-NANO and BLC-EVP-NANO had reduced the HCT116 invasion, when compared to the untreated and ETP treated cells which indicate the major role of BLC and EVP included in the NE formula. The EVP is a valuable source of linoleic acid and gamma-linolenic acid. The gamma-linolenic acid causes an increase in the expression of the nm-23 metastasis-suppressor gene in cancer cells, which promotes the inhibition of angiogenesis, cancer cell migration, and subsequently, cancer metastasis[27,20].

In conclusion, a novel nanoemulsion formula BLC-EVP-NANO was designed by combining natural oils, Ribes nigrum (black currant) seed oil (BLC), and organic evening primrose oil (EVP) with an emulsifying agent. Incorporating ETP into a new formula had augmented its anti-proliferation effect on HCT116 colon cancer cells. The combination of ETP with the natural oils in ETP-BLC-EVP-NANO had enhanced the induction of apoptosis and the inhibition of the invasion capability among colon cancer cells. According to our findings, molecular mechanisms of the anticancer activity of the BLC-EVP-NANO and ETP-BLC-EVP-NANO formulas need to be studied and further investigations in animal models are also required.

Conflict of Interest:

The authors declare that they have no conflict of interest.

REFERENCES


